

# Short-term Effects of Botulinum Toxin A and Serial Casting on Triceps Surae Muscle Length and Equinus Gait in Children with Cerebral Palsy

Vliv léčby botulinum toxinem-A a redresního sádrování na délku musculus triceps surae a ekvinózní postavení nohy během chůze u pacientů s dětskou mozkovou obrnou

## Abstract

**Aims:** The aim of the study was to perform a comprehensive analysis of the short-term effects of a standardized high dose of BTX-A and serial casting on spastic equinus in children with cerebral palsy. A second goal was to evaluate this short-term effect on muscle lengths of the triceps surae. **Materials and methodology:** Prospective study on 10 children (17 limbs) with spastic cerebral palsy and equinus gait pattern. Three-dimensional kinematic and kinetic gait analysis with musculo-skeletal modelling was used to evaluate pre- and 10 weeks post-treatment results. The paired Student's T-test was used for data analysis. **Results:** Walking velocity and stride length did not change after BTX-A application. The maximal ankle angle at the end of single support increased ( $p = 0.045$ ) which led to a change of the ankle angle slope quotient towards normal positive values ( $p = 0.001$ ). Abnormal ankle power generation in the first part of single stance changed towards normal ( $p = 0.012$ ). Notably, the ankle plantar-flexor power was not reduced 10 weeks after BTX-A injection ( $p = 0.486$ ). No lengthening of the triceps surae muscles compared to the baseline assessment was found. **Conclusions:** Beneficial functional changes in ankle kinematics and kinetics after the application of BTX-A when combined with serial casting were demonstrated. The results of our study underline the possible differences in effect of BTX-A on intrafusal and extrafusal muscle fibres.

## Souhrn

**Cíle:** Cílem této studie bylo provést komplexní analýzu krátkodobého účinku vysokodávkovaného botulinum toxinu-A (BTX-A) aplikovaného společně s redresním sádrováním z důvodu ekvinózního postavení nohy během chůze u pacientů s dětskou mozkovou obrnou (DMO). Dalším cílem bylo hodnotit vliv této léčby na délku musculus triceps surae. **Materiál a metodika:** Jedná se o prospektivní studii, do které bylo zařazeno 10 pacientů (17 končetin) se spastickou formou DMO a ekvinózním postavením nohy. K hodnocení byla použita metoda trojdimenzionální kinematické a kinetické analýzy chůze společně s počítačovou modelací délky musculus triceps surae. Pacienti byli vyšetřeni před a 10 týdnů po léčbě. Ke statistické analýze byl použit párový t-test. **Výsledky:** Rychlost chůze a délka kroku se po aplikaci BTX-A nezměnila. Maximální dorziflexe na konci fáze jedné opory se zvýšila ( $p = 0,045$ ), což vedlo k normalizaci „slope quotient“ ( $p = 0,001$ ). Došlo také k odstranění patologické generace síly během první poloviny fáze jedné opory ( $p = 0,012$ ). Oproti očekávání, síla plantiflexorů nebyla aplikací BTX-A ovlivněna ( $p = 0,486$ ). Neprokázáni jsme prodloužení musculus triceps surae. **Závěr:** Aplikace BTX-A společně s redresním sádrováním vede ke zlepšení kinematiky a kinetiky chůze pacientů s ekvinózní deformitou a DMO. Výsledky naší studie upozorňují na možnost rozdílného působení BTX-A na intrafuzální a extrafuzální svalová vlákna.

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Accepted for review: 15. 7. 2009  
Accepted for publication: 21. 8. 2009

## Klíčová slova

cerebral palsy – botulinum toxin A – pes equinus – gait analysis

## Key words

dětská mozková obrna – botulinum toxin-A – pes equinus – analýza chůze

## Introduction

Cerebral palsy refers to a group of disorders in the development of posture and motor control, occurring as the result of a non-progressive lesion of the developing central nervous system [1]. Children with cerebral palsy may display a range of movement disorders, alone or in combination, including dystonia, athetosis, ataxia and spasticity [2]. Equinus gait is one of the most common motor manifestations of muscle spasticity in cerebral palsy [3]. Equinus decreases stability during the stance phase of gait, interferes with the smooth translation of the body over the foot and leads to inadequate clearance of the foot in the swing phase. [4]. If untreated, protracted spasticity can lead to fixed muscle contractures that may require surgical intervention.

Previous reports have found that the presence of spasticity increases muscle stiffness and thereby inhibits muscle growth [4,5]. Besides conservative therapies such as physiotherapy, serial casting, orthotics and oral medication, a variety of invasive treatment methods are now commonly available to manage spasticity in cerebral palsy. These include selective dorsal rhizotomy (SDR), intrathecal administration of baclofen (ITB) or botulinum toxin type A (BTX-A) injections, which has been used clinically for more than 20 years. BTX-A induces muscle weakness by preventing the release of acetylcholine from the presynaptic axon at the motor endplate [5]. The degree of weakening depends on the dose of BTX-A and on the number of synapses affected [6]. Spasticity reduction due to the effects of BTX-A injections typically lasts from 12 to 16 weeks. Re-innervation takes place by sprouting of new nerve terminals, a process that peaks at 60 days in humans [7]. Functional benefits may last for up to six months or even longer [8]. In addition to

the effect of muscle weakening, BTX-A has been shown to influence the longitudinal growth of an injected muscle in an animal model [9]. Based on computer simulation and modelling, the same effect was confirmed in humans four weeks after BTX-A application [10].

The motivation for the present study was to perform a comprehensive analysis of the short-term effects of a standardized dose of BTX-A and serial casting on spastic equinus in children with cerebral palsy. A second goal was to evaluate this short-term treatment on muscle length of the triceps surae. To evaluate functional outcome and changes in muscle length, we applied three-dimensional gait analysis and calculated individual dynamic peak muscle lengths by using musculo-skeletal modelling techniques.

## Methods

### Design

The study is a prospective analysis of the short-term effects of a standardized high dose of BTX-A (7 IU/kg) applied to the gastro-soleus complex and serial casting. The patients were examined before and 10.1 weeks (SD 1.3) after a BTX-A application. The pre-treatment gait analysis was used as a baseline for validation of treatment effect.

### Subjects

For this investigation, equinus gait was defined as a peak ankle dorsal-flexion of more than one standard deviation below the normal average during the stance phase of gait [11]. Inclusion and exclusion criteria are listed in Table 1. Based on these criteria, 10 children with spastic cerebral palsy were included in the trial (4 males, 6 females). The average age of our study group was 7 years and one month (SD 2 years and 3 months). Seven children were diplegic and three hemiple-

gic. A total of 17 lower extremities were analysed and used for statistical analysis. The ethics committee of the local medical university approved the study.

### Intervention

BTX-A injections were performed under general anaesthesia. A BTX-A dose of 7 IU/kg (Botox®, Allergan Inc, Irvine, CA, USA) was applied to multiple sites over the muscle belly of the gastrocnemius and soleus. A multiple injection site technique was applied in which every site was injected with 10 IU BTX-A. The positioning of the needle in the muscle was as described by Baker et al [10]. A few hours after the BTX-A injections a below-knee walking cast was applied in maximal ankle dorsal-flexion for a duration of three weeks. Casts were changed every week. Special physiotherapy training was performed after the removal of the third cast in all cases, on an out-patient basis two times a week for the whole period of the study. The physiotherapy included passive muscle stretching and gait improvement training; either the Vojta concept or the Bobath concept was utilized.

### Gait analysis

Computerized gait analysis was performed using a six-camera, video-based motion-capturing system (Vicon MX, Oxford Metrics, Oxford, U.K.) and four floor-mounted force plates (Kistler Instruments Limited, Winterthur, Switzerland). Thirteen reflective markers were used to define the pelvis and lower extremity segments in accordance with the Vicon Clinical Manager model (Oxford Metrics, Oxford, U.K.). Moment and power parameters were normalized to the weight of the patients. Power generation and absorption patterns in the sagittal plane were calculated and labelled according to the method described by Winter [12]. All pa-

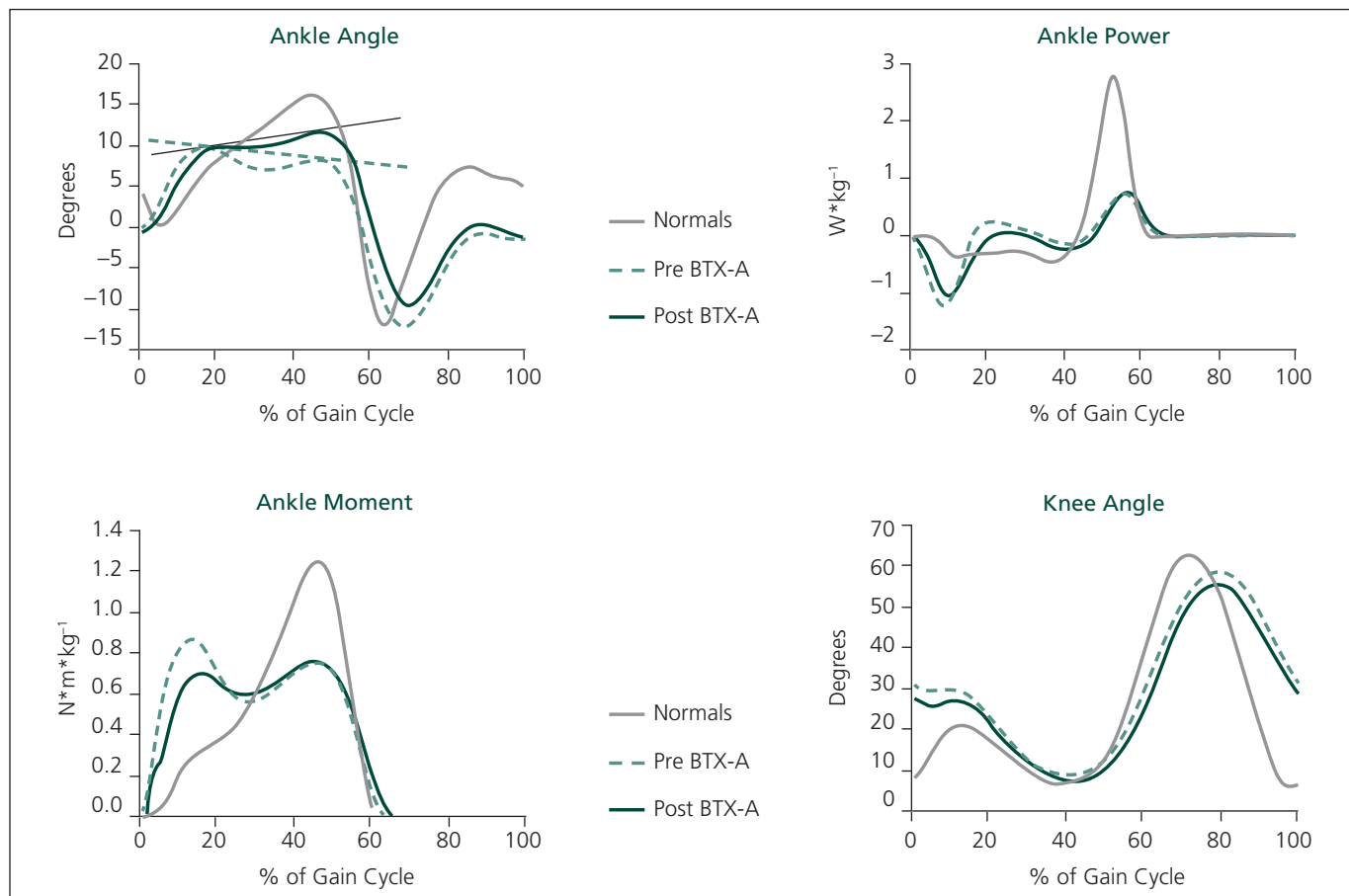
**Table 1. Inclusion and exclusion criteria.**

#### Inclusion criteria

1. Spastic diplegic or hemiplegic cerebral palsy
2. Equinus gait
3. Ability to walk at least 12 m without walking aids
4. Gross Motor Function Classification System Level I-II
5. Good vision and willingness to participate
6. Complete gait analysis data sets to perform musculo-skeletal modelling

#### Exclusion criteria

1. Previous surgery of the triceps surae
2. Botulinum toxin A treatment within six months before entering the trial
3. Dystonic, athetotic or ataxic form of cerebral palsy



**Figure 1. Sagittal plane ankle and knee kinematics and kinetics plots over the gait cycle.**

*Ankle Angle:* the straight lines in the Ankle Angle graph show the slope quotient pre- and post botulinum toxin A application. A rising "slope quotient" indicates improvement of ankle motion. There is an obvious improvement to normal positive values of slope quotient.

*Ankle Moment:* there is a decrease in abnormal ankle moment during the first part of the single stance phase.

*Ankle Power:* decrease of abnormal power generation in the first part of the single stance phase.

*Knee Angle:* there is no significant difference.

(Normals: normally developing children; Pre-BTX-A: patients with cerebral palsy before the botulinum toxin A application; Post BTX-A: patients with cerebral palsy after botulinum toxin A application)

tients walked at self-selected speeds along a 12-metre walkway. For each patient a minimum of five trials, providing clear foot-force plate contact, were captured and averaged. To better describe the different patterns of ankle kinematics during the single stance phase, a "slope quotient" was employed [13]. The slope quotient of the sagittal plane ankle angle during walking was computed as a subtraction of the ankle angle at the beginning of single support from the ankle angle at the end of the single support. Positive values of the slope quotient indicate muscle elongation, negative values indicate muscle shortening and values close to zero show that a muscle has stayed at the same length during the single support phase of the gait cycle.

#### Muscle length calculation

Based on kinematic data, Mobile GaitLab software (Duisburg-Essen University, Institute of Mechatronics and System Dynamics, Germany) [14] was used to compute individual muscle lengths of the gastrocnemius and soleus. The specification of the lower extremity architecture was based on the origin and insertion coordinate data compiled by Yamaguchi [15]. The model defines the musculoskeletal geometry of a normal adult male. Three-dimensional musculo-tendon (MT) pathways were modelled as a series of straight-line segments extending from origin to insertion. Where appropriate, the MT pathways were sub-sectioned into a number of straight-line segments by introducing via-points. Musculo-tendon length para-

meters were normalized to allow comparison between subjects.

#### Statistics

Ankle and knee kinematic and kinetics in the sagittal plane as well as maximal length of the medial gastrocnemius (MGAC), lateral gastrocnemius (LGAC) and the soleus (SOL) muscles over the gait cycle were considered as main outcome measures for this study. Student's T-test (Statistica 6.0, StatSoft, Tulsa, OK) was used to describe the pre- and post-treatment differences.

#### Results

The walking velocity and the stride length did not change after the BTX-A application. Ankle kinematics and kinetics changed towards normal 10 weeks after the treatment

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Table 2. Summary of results

|   | p     | Pre-BTX |         |         |        | Post-BTX |         |         |        |
|---|-------|---------|---------|---------|--------|----------|---------|---------|--------|
|   |       | Mean    | CI 5%   | CI 95%  | SD     | Mean     | CI 5%   | CI 95%  | SD     |
| Slope quotient  | 0.001 | -0.489  | -2.234  | 1.256   | 3.394  | 4.226    | 1.997   | 6.454   | 4.335  |
| Maximal ankle angle at the end of single support (°)                                    | 0.045 | 6.739   | 3.836   | 9.642   | 5.646  | 11.016   | 7.781   | 14.250  | 6.291  |
| Timing of maximal ankle angle (% of gait cycle)   | 0.003 | 28.412  | 21.134  | 35.690  | 14.156 | 42.765   | 36.469  | 49.061  | 12.245 |
| Maximal ankle moment (N × m × kg <sup>-1</sup> )  | 0.362 | 0.921   | 0.807   | 1.035   | 0.221  | 0.854    | 0.749   | 0.958   | 0.203  |
| Timing of maximal ankle moment (% of gait cycle)  | 0.024 | 23.000  | 15.085  | 30.915  | 15.395 | 35.588   | 27.608  | 43.568  | 15.520 |
| Maximal power generation in the first part of single support (Watt × kg <sup>-1</sup> ) | 0.012 | 0.300   | 0.181   | 0.419   | 0.232  | 0.094    | -0.017  | 0.206   | 0.216  |
| Maximal power generation over the gait cycle (Watt × kg <sup>-1</sup> )                 | 0.486 | 0.998   | 0.829   | 1.166   | 0.328  | 0.914    | 0.728   | 1.100   | 0.362  |
| Maximal knee flexion (°)  | 0.162 | 58.733  | 55.566  | 61.900  | 6.159  | 55.169   | 50.944  | 59.393  | 8.216  |
| Maximal knee extension (°)  | 0.747 | 7.614   | 4.251   | 10.977  | 6.541  | 6.897    | 3.672   | 10.123  | 6.273  |
| Maximal length of medial gastrocnemius (% of normalized muscle length)                  | 0.128 | 101.746 | 101.572 | 101.920 | 0.314  | 102.101  | 101.823 | 102.379 | 0.502  |
| Maximal length of lateral gastrocnemius (% of normalized muscle length)                 | 0.930 | 102.494 | 102.036 | 102.952 | 0.827  | 102.518  | 102.177 | 102.859 | 0.616  |
| Maximal length of soleus (% of normalized muscle length)                                | 0.385 | 101.863 | 101.585 | 102.142 | 0.503  | 101.998  | 101.825 | 102.171 | 0.312  |

The table summarizes the results of pre- and post- botulinum toxin A application analysis of ankle and knee kinematics, kinetics and musculotendon lengths of triceps surae. Significant changes in the ankle kinematics document an improvement after BTX-A application. Not only the abnormal power generation in the first part of single support phase of stance normalized, but there was no decrease in maximal power generation, which is the most important factor for forward propulsion in walking. No change in muscle lengths was observed after BTX-A application. (p: level of statistical significance, CI: confidence interval, SD: standard deviation)

(Fig. 1). The maximal ankle angle at the end of single support increased ( $p = 0.045$ ) and also the timing of the maximal angle shifted towards normal values (Table 2). The ankle angle slope quotient changed to normal positive values ( $p = 0.001$ ). We did not observe any changes in knee kinematics. While the maximum ankle moment values remained unchanged, the abnormal ankle moment peak in the first part of the single support phase decreased and the timing of maximum ankle moment occurred later in the stance phase ( $p = 0.024$ ). An abnormal power generation in the first part of the single support stance phase decreased markedly ( $p = 0.012$ ). Musculo-skeletal modelling revealed no lengthening of the triceps surae muscles compared to the baseline assessment (Table 2). We did not observe any adverse effects in our study group.

### Discussion

This study utilised three-dimensional gait analyses to evaluate the effects of BTX-A

and serial casting on kinematic and kinetic gait parameters in children with cerebral palsy who exhibit equinus gait. Short-term effects were analysed ten weeks after BTX-A injections. To evaluate changes in dynamic muscle length, musculo-skeletal modelling techniques were applied. The results of this study confirm previously reported beneficial short-term outcome when equinus gait is treated with BTX-A and serial casting in children with cerebral palsy. Like other authors [7,16] we observed significant improvements of ankle kinematics and kinetics. These improvements include a reduction in equinus and a change of timing and modulation of ankle motion patterns towards normal. During the "second rocker" of ankle motion we documented improved dorsal flexion at the end of the stance phase of the gait cycle [4]. As it has been demonstrated that equinus gait increases the energy expenditure during walking in children with cerebral palsy [17], the improvement of

the ankle kinematics might allow for longer walking distances, which could improve the quality of life. The changes in ankle moments and powers observed in this study provide insight into the underlying patho-physiology of the gastro-soleus muscle in spastic equinus gait. Abnormal power absorption was observed whenever a forefoot landing occurred and the ankle was loaded through a forefoot lever. This power absorption can be interpreted as a calf muscle stretch, which is followed by a burst of power generation in the first half of single support. This burst of power generation points towards a spasticity-driven stretch reflex after loading the ankle via a forefoot lever arm. When treated with BTX-A and serial casting the reflex-induced power generation was markedly reduced. In this study, musculo-skeletal modelling revealed no changes in muscle length that could be attributed to the interventions of BTX-A and serial casting. This finding contrasts with previous reports [10,18,19]

that documented changes in calf muscle length as a beneficial short-term outcome. As the changes in kinematics and kinetics cannot be attributed to changes in muscle length, possibly BTX-A affects intrafusal muscle spindles, reducing the effects of the gamma-loop stretch reflex. In a recent study of the long-term effects of BTX-A treatment on muscle tone and range of motion in a group of children with cerebral palsy, Tedroff et al [20] demonstrated that BTX-A was efficient in reducing the muscle tone but the improvement of range of motion lasted for only a short period of time in the gastrocnemius muscle. This evidence would support our conclusion that during the first weeks after the application of BTX-A, the therapy might have a more significant influence on muscle spasticity than on muscle growth. On the other hand, Kanovsky et al showed a lack of deterioration in maximum passive ankle dorsiflexion for both groups in a paper concerning the long-term efficacy and tolerability of 4-monthly versus yearly BTX-A treatment for lower limb spasticity in children with cerebral palsy [21].

The dose of BTX-A used in this trial (7 IU/kg of BTX-A for the triceps surae complex) is rather high when compared in the literature [22,23]. However, a randomized, double-blinded trial demonstrated that high-dose BTX-A treatment has a better effect on gait and spasticity improvement than low-dose BTX-A treatment [24]. Similar dosages of BTX-A have been evaluated by other authors [7,25] who did not observe any increase in adverse effects. There is no general agreement on the use of serial casting together with BTX-A treatment in children with cerebral palsy [26]. It has been shown that serial casting enhanced and prolonged the effect of BTX-A treatment [7,16]. In a more recent study, Newman et al [27] showed additional benefits in the recurrence of spasticity when casting is delayed after BTX-A injections. Based on these supportive data and our personal experience, we adopted this procedure for routine use. The cast is not applied immediately after BTX-A administration but on the same day (approximately four to five hours after injecting BTX-A). This time is used to move and stretch the triceps surae muscle. It has been proved in an animal model that as few as 10 passive stretch/relax cycles can increase the efficacy of BTX-A [28]. However, to the best

of our knowledge, no published data confirms this finding in a group of children with cerebral palsy. On the other hand, electrical stimulation has been proved to prolong gait improvement in children with spastic diplegic cerebral palsy [29].

Management of cerebral palsy is primarily directed towards maintaining or regaining muscle length. Use of BTX-A here is based on the concept that muscle fibres in children with spastic cerebral palsy are short, and weakening the muscles with BTX-A injections might allow them to be stretched and thus grow in length. Thus the progression from dynamic to fixed deformity may be delayed [30] and any orthopaedic surgical procedures might be postponed or reduced in frequency [31]. Although muscle growth following BTX-A injection has also been found in animal models [9,32], the findings of our study did not support this in children with cerebral palsy in a short-term follow up. As there is no direct way to measure muscle length in humans, muscle length calculations are based on mathematical models of the lower extremities and on measurements of ankle, knee, hip and pelvis kinematics. It is obvious that such mathematical modelling approaches have limitations, but the method is well accepted in the literature [25,33] because it provides additional information which can help us to better understand the biomechanics of a spastic muscle. We speculate that a period of ten weeks is too short to expect any measurable gain in muscle length by muscle growth. However, we observed significant improvements in ankle kinematics and kinetics. We interpret the beneficial changes in kinematics and kinetics observed in this study as an effect of BTX-A on intrafusal muscle fibres [34]. Therefore, the application of BTX-A may have a more significant influence on muscle spasticity than on muscle growth. The BTX-A is effective in reducing the over-activity of the spastic muscle and improving its function [35]. Moreover, even if the main effect of BTX-A might be to weaken the muscle, we observed no decrease in power generation in terminal stance, which is the most important factor for forward propulsion in walking. Again, this could be explained by different influences of BTX-A on intrafusal and extrafusal muscle fibres. Such differences in outcome might be attributed to the variety of methods used

to calculate muscle lengths in the various studies.

In conclusion, this study demonstrated beneficial functional changes in ankle kinematics and kinetics after the application of BTX-A when combined with serial casting. We did not observe any change in the peak muscle-tendon length of the gastro-soleus muscle complex. Further studies are needed to address the question of muscle growth after BTX-A application in children with spastic cerebral palsy.

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